

Learning sparsifying filter banks

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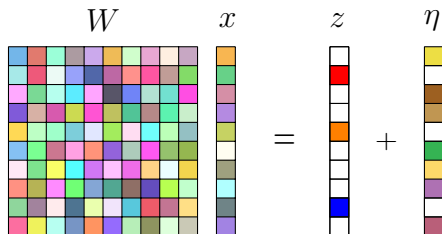
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The Problem

$$y = Ax + e$$

- $x \in \mathbb{R}^{N^2}$: Desired image
- $y \in \mathbb{C}^M$: Measurements
- $A \in \mathbb{C}^{M \times N^2}$: System operator
- $e \in \mathbb{C}^M$: Noise
- Underdetermined or ill-conditioned \implies must incorporate prior information!
 - ▶ Assume signal has sparse representation

Transform Sparsity



- $W \in \mathbb{R}^{N_c \times K^2}$: Sparsifying transform
- $Wx \approx \text{sparse}$
- W is left-invertible: $x \approx W^\dagger z$

Transform Sparsity

$$z^* = \min_z \frac{1}{2} \|Wx - z\|_2^2 + \nu \|z\|_0$$

$$z_i^* = \begin{cases} [Wx]_i & |[Wx]_i| \geq \sqrt{\nu} \\ 0 & \text{else} \end{cases}$$

$$\triangleq \mathcal{T}_\nu(Wx)$$

Analytic Sparse Models

- Designed for optimal properties on a mathematical class of signals
- Fast implementation
- Hard to design for high dimensional data

Adaptive Sparse Models

- Learn a good representation directly from data
 - ▶ Minimize objective function over training set
- Synthesis sparsity: Dictionary learning
- Transform sparsity: Transform learning

Transform Learning

$$\min_{W,Z} \frac{1}{2} \|WX - Z\|_F^2 + \nu \|Z\|_0 + J(W)$$

- X : Training data
- Z : Sparsified data
- J : Encourages well conditioned, left-invertible W

Transform Learning Algorithms

$$\min_{W,Z} \frac{1}{2} \|WX - Z\|_F^2 + \nu \|Z\|_0 + J(W)$$

- Algorithms to learn square, tall, separable, block structured ...
- Applications to image denoising, magnetic resonance imaging (MRI), computed tomography...
- Training set usually consists of patches of image or video data

Patches

1	2	3	4	5	6
7	8	9	10	11	12
13	14	15	16	17	18
19	20	21	22	23	24
25	26	27	28	29	30
31	32	33	34	35	36

Patches

1	2	3	4	5	6
7	8	9	10	11	12
13	14	15	16	17	18
19	20	21	22	23	24
25	26	27	28	29	30
31	32	33	34	35	36

1
2
7
8

x_1

Patches

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7	8	9	10	11	12
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31	32	33	34	35	36

1	2
2	3
7	8
8	9

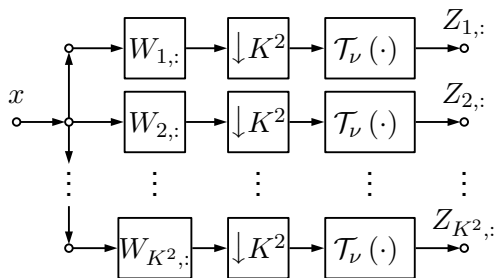
x_1 x_2

From Patches To Filter Banks

Non-overlapping Patches

1	2	3	4	5	6
7	8	9	10	11	12
13	14	15	16	17	18
19	20	21	22	23	24
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Sparsifying Transforms as Filter Banks



Sparsifying Transforms as Filter Banks

- $\text{vec}(WX) = \mathcal{H}_W x$
- W is the **polyphase matrix** of a filter bank
- **Defn:** \mathcal{H}_W is perfect reconstruction (PR) if \mathcal{H}_W left invertible (LI).
- Properties of filter bank controlled by patch extraction and by W
 - ▶ Shape of patches \rightarrow shape of filters
 - ▶ Rows of $W \rightarrow$ channels of filter bank
 - ▶ \mathcal{H}_W is PR $\Leftrightarrow W$ is LI

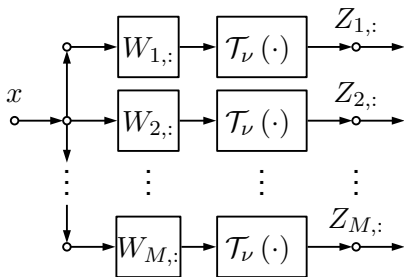
Sparsifying transforms as filter banks

- Take away: Existing transform learning algorithms learn perfect reconstruction downsampled filter banks!
 - ▶ ...but we usually use overlapping patches.
- Requiring W to be LI is stronger than requiring \mathcal{H}_W to be PR!
- Two questions:
 - 1 Do we benefit by requiring \mathcal{H}_W to be PR and relaxing the LI condition on W ?
 - 2 Can we find an efficient algorithm to learn such a \mathcal{H}_W ?

Previous Work

- Connection between patch based analysis operators and convolution previously known
- Convolution often used as a computational tool
- (Cai, 2014) learned a PR filter bank by requiring $W^T W = I$

Maximally Overlapping Patches



- Maximally overlapping patches
- W is no longer the polyphase matrix for \mathcal{H}_W
- Generally difficult to check the PR condition

Maximally overlapping Patches

- Simplify: replace linear convolution with circular convolution
- Patch interpretation: 'wrap around' image boundary
- Third representation
 - ▶ C_j : 2D circulant matrix such that $C_j x = w_j \circledast x$
 - ▶ $C_W \triangleq [C_{w_1}^T, C_{w_2}^T, \dots, C_{w_{N_C}}^T]^T$
 - ▶ $C_W x = \mathcal{H}_W x = \text{vec}(WX)$
 - ▶ C_W is highly structured: block-circulant with circulant blocks

A few ingredients...

- $\Phi \in \mathbb{C}^{N^2 \times N^2}$: Normalized 2D discrete Fourier transform (DFT) matrix.
- $\bar{\Phi} \in \mathbb{C}^{N^2 \times K^2}$: Zero-padded DFT of $K \times K$ signal
- $\mathbf{1}_k \triangleq \underbrace{[1, 1, \dots, 1]^T}_{k \text{ entries}}$
- $C_j = \Phi^H \text{ddiag}(\bar{\Phi} W_{j,:}^T) \Phi$

The Key Property

- Each frequency must pass through at least one channel!

Diagonalization

$$C_W^T C_W = \Phi^H \text{ddiag} \left(\left| \bar{\Phi} W^T \right|^2 \mathbf{1}_{N_c} \right) \Phi$$

Perfect Recovery Condition

\mathcal{H}_W is PR \Leftrightarrow each entry of $\left| \bar{\Phi} W^T \right|^2 \mathbf{1}_{N_c} > 0$

- Decouples the choice of N_c and K
- Especially attractive for high dimensional data

Learning a sparsifying filter bank

Learning Formulation

- Desiderata

- ▶ Parameterize with few degrees of freedom
- ▶ $\mathcal{H}_W x$ should be (approximately) sparse
- ▶ \mathcal{H}_W should be PR and well conditioned
- ▶ No identically zero filters
- ▶ No duplicated filters

Learning Formulation

- WX should be (approximately) sparse

$$F(W, Z, x) \triangleq \frac{1}{2} \|WX - Z\|_F^2 + \nu \|Z\|_0$$

Learning Formulation

- \mathcal{H}_W should be PR and well conditioned
- No uniformly zero filters

$$J_1(W) = \left\| \left| \bar{\Phi} W^T \right|^2 \mathbf{1}_{N_c} - \mathbf{1}_{N^2} \right\|_2^2 - \beta \sum_{j=1}^{N_c} \log \left(\|W_{j,:}\|_2^2 \right)$$

Learning Formulation

- No duplicated filters

$$J_2(W) = \sum_{1 \leq i < j \leq N_c} -\log \left(1 - \left(\frac{\langle W_{i,:}, W_{j,:} \rangle}{\|W_{i,:}\|_2 \|W_{j,:}\|_2} \right)^2 \right)$$

Learning Formulation

$$\min_{W, Z} \frac{1}{2} \|WX - Z\|_F^2 + \alpha J_1(W) + \gamma J_2(W) + \nu \|Z\|_0$$

Alternating minimization:

- $Z^{k+1} = \arg \min_Z \frac{1}{2} \|W^k X - Z\|_F^2 + \nu \|Z\|_0$
- $W^{k+1} = \arg \min_W \frac{1}{2} \|WX - Z^{k+1}\|_F^2 + \alpha J_1(W) + \gamma J_2(W)$

Alternating Minimization

$$Z^{k+1} = \arg \min_Z \frac{1}{2} \|WX - Z\|_F^2 + \nu \|Z\|_0$$

- Closed form: $Z^{k+1} = \mathcal{T}_\nu(WX)$

Alternating Minimization

$$W^{k+1} = \arg \min_W \frac{1}{2} \|WX - Z\|_F^2 + \alpha J_1(W) + \gamma J_2(W)$$

- Minimize using L-BFGS

Application to Magnetic Resonance Imaging

Imaging Model

- Imaging Model: Undersampled Fourier measurements

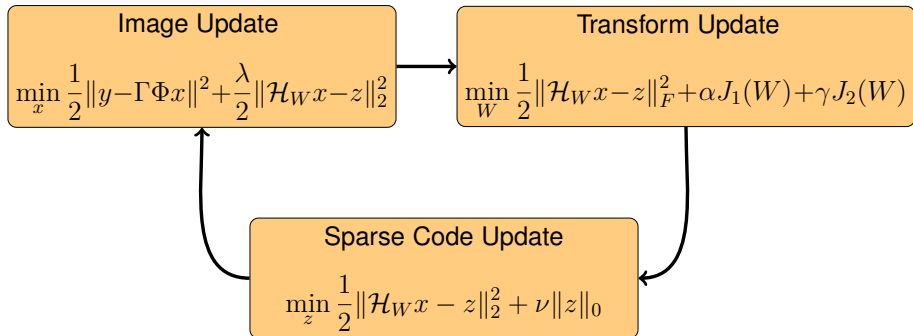
$$y = \Gamma\Phi x + e$$

- $x \in \mathbb{R}^{N^2}$: Input image
- $\Phi \in \mathbb{C}^{N^2 \times N^2}$: DFT matrix
- $\Gamma \in \mathbb{C}^{M \times N^2}$: Row selection matrix
- $e \in \mathbb{C}^M$: Zero mean Gaussian noise

Image Reconstruction

$$\min_{x, \mathcal{H}_W, z} \frac{1}{2} \|y - \Gamma \Phi x\|_2^2 + \lambda \left(\frac{1}{2} \|\mathcal{H}_W x - z\|_2^2 + \nu \|z\|_0 + \alpha J_1(\mathcal{H}_W) + \gamma J_2(\mathcal{H}_W) \right)$$

- Data fidelity
- Transform learning
- Solve using alternating minimization

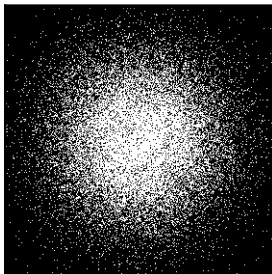
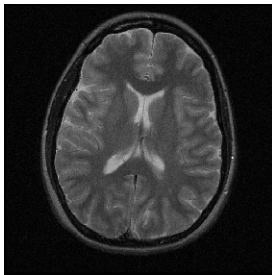


Experiments

- Synthetic MR data from magnitude image
- ≈ 5 fold undersampling
- Vary filter size & number of channels
- Compare against square patch-based transform learning:

$$\min_{W,x,Z} \frac{1}{2} \|y - \Gamma \Phi x\|_2^2 + \frac{\lambda}{2} \|WX - Z\| + \nu \|Z\|_0 \\ + \alpha \|W\|_F^2 - \beta \log \det W$$

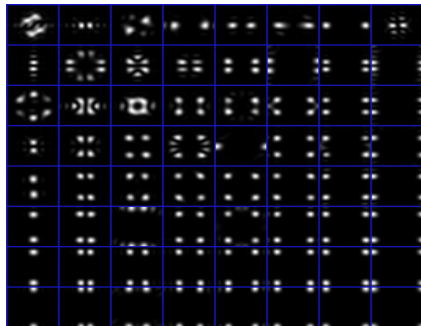
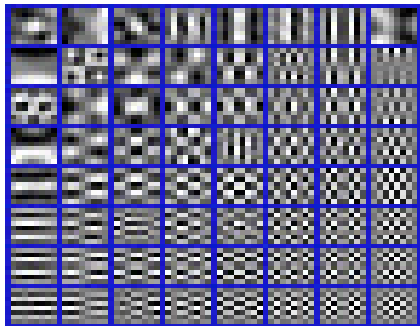
- Solved using alternating minimization
- Initialized with DCT matrix



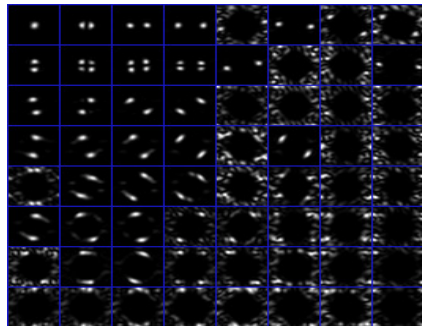
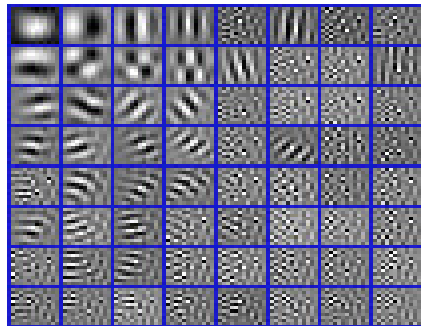
Reconstruction PSNR (dB)

σ / PSNR In	Filter Bank			Patch Based
	$N_c = 64$ $K = 8$	$N_c = 128$ $K = 8$	$N_c = 64$ $K = 12$	64×64
0 / 29.6	35.2	35.2	35.1	34.6
$\frac{10}{255}$ / 28.8	32.6	32.7	32.6	32.5
$\frac{20}{255}$ / 26.9	31.6	31.6	31.2	31.3

Learned filters 8×8



Learned filters 12×12



Conclusion

Conclusion

- New framework for learning filter bank sparsifying transforms
- Replace patch recovery conditions with image recovery
- Decouples number of channels from filter length
- Outperforms patch based transform for MR reconstruction

Conclusion

- Extended version on ArXiv soon!
- For more on transform learning
 - ▶ Sai Ravishankar's talk (Tuesday Afternoon)
 - ▶ <http://transformlearning.csl.illinois.edu>
 - ▶ <http://lukepfister.me>
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